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Spatiotemporal Evolution of Temperature During Transient Heating of Nanoparticle Arrays

Nanoparticles (NPs) are promising agents to absorb external energy and generate heat. Clusters of NPs or NP array heating have found an essential role in several biomedical applications, diagnostic techniques, and chemical catalysis. Various studies have shed light on the heat transfer of nanostructures and greatly advanced our understanding of NP array heating. However, there is a lack of analytical tools and dimensionless parameters to describe the transient heating of NP arrays. Here we demonstrate a comprehensive analysis of the transient NP array heating. Firstly, we develop a set of analytical solutions for the NP array heating and provide a useful mathematical description of the spatial-temporal evolution of temperature for 2D, 3D, and spherical NP array heating. Based on this, we introduce the concept of thermal resolution that quantifies the relationship between minimal heating time, NP array size, energy intensity, and target temperature. Lastly, we define a set of dimensionless parameters that characterize the transition from confined heating to delocalized heating. This study advances the understanding of nanomaterials heating and guides the rational design of innovative approaches for NP array heating. [DOI: 10.1115/1.4053196]

Keywords: nanoparticle array heating, thermal resolution, heating overlap, confined heating, delocalized heating

Introduction

Nanoparticles (NPs) have been applied as nanoscale heaters in a variety of applications [1-4], including thermal therapy [5-8], droplet heating [9], drug delivery [10-12], neuromodulation [13,14], photoacoustic imaging [15,16], photothermal imaging [17,18], and photothermal catalysis [19-21]. For these applications, precise control of both the magnitude and spatiotemporal distribution of the temperature is often crucial [22,23]. As an example, neuromodulation via the thermally sensitive ion channel TRPV1 requires a threshold temperature to activate the channel $(40 \,^{\circ}\text{C}-53 \,^{\circ}\text{C})$ [24–26], while overheating (>60 $^{\circ}\text{C}$) can lead to cellular damage [27]. Additionally, for molecular hyperthermia, highly localized heating at the nanoscale is essential for targeted protein inactivation [28-30]. Therefore, a comprehensive understanding of NP heating is particularly valuable when optimizing the spatiotemporal evolution of the temperature profile for these applications. While single NP heating has been extensively investigated and is well understood [30-35], NP cluster or NP array heating is far from well understood due to the complexity of interactions among NPs and the diversity of possible NP array geometries.

Despite the inherent complexity of NP array heating, various works have shed light on the phenomena. For example, numerical and experimental investigations demonstrated that NP cluster heating may lead to a significantly larger temperature rise as compared to single NP heating, with the temperature rise for NP clusters increasing with NP concentration [36–41]. Additionally, efforts have been made to determine analytical solutions for NP array heating. Keblinski et al. Derived a temperature function of 3D NP array heating under steady-state [42]. They demonstrated that the array size and NP concentration determine the array temperature rise, which could be orders of magnitude higher than that

In this report, we systematically analyzed the transient heating process for NP arrays. First, we derived a set of analytical temperature functions that predict the temperature rise for three representatives NP assemblies (2D, 3D, and spherical NP arrays (Fig. 1)), alleviating the need to run costly numerical simulations. Next, we developed the concept of thermal resolution to quantify the minimal size and heating time required for an NP array to reach a specified target temperature rise at a given heating intensity, therefore providing guidelines on physical limitations for applications based on NP array heating. Lastly, we defined a new set of

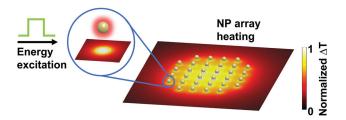


Fig. 1 Schematic illustrations of nanoparticle (NP) array. Absorption of external energy excitation and conversion into heat by NP arrays.

of single NP heating due to heating overlap between NPs in the array. Baffou et al. further derived temperature functions for 1D and 2D NP array heating under steady-state and repeated femtosecond pulsed excitations [43,44]. Importantly, Baffou et al. described sets of dimensionless parameters that characterize the transition from confined heating to delocalized heating defined based on the temperature functions [44]. Although these seminal works have improved our understanding of NP array heating under the steady-state, a detailed description of transient NP array heating is lacking. Meanwhile, applications based on NP array heating under single pulsed heating with duration ranging from nanoseconds to minutes have been reported recently [24,29,45]. Consequently, an analysis of the spatiotemporal evolution of temperature during transient array heating is urgently needed.

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dimensionless parameters based on the interparticle distance and heating time to characterize the transition from confined heating to delocalized heating. From analysis based on these dimensionless parameters, we found that for spherical NP arrays, delocalized heating first occurs along the spherical surface, and then further delocalizes throughout the volume inside the sphere. This effect may be particularly relevant when heating NP arrays on the surface of a nanovesicle or living cell [10]. This work provides clear analytical guidance for designing innovative approaches that utilize NP heating under realistic physical constraints.

Methods

Temperature Function for Single Nanoparticle Heating. We start by considering single NP heating. Many of the applications of NP heating mentioned above are based on heating metallic NPs in an aqueous solution. In these cases, NPs absorb external energy excitations, such as laser irradiation [46], magnetic [47], or ultrasonic fields [48], and convert that energy into heat (Fig. 1) [1]. For a single NP, this nanoscopic absorption-heating process can be modeled by treating the NP as a spherical particle subject to volumetric heating and heat transfer into a surrounding homogeneous aqueous medium using an application of Fourier's law

$$\begin{cases} \frac{1}{r^2} \frac{\partial}{\partial r} \left(r^2 \frac{\partial T}{\partial r} \right) + \frac{q_v}{k_{\rm NP}} = \frac{1}{\alpha_{\rm NP}} \frac{\partial T}{\partial t}, & 0 \le r < r_{\rm NP}, \ t \ge 0 \\ \frac{1}{r^2} \frac{\partial}{\partial r} \left(r^2 \frac{\partial T}{\partial r} \right) = \frac{1}{\alpha} \frac{\partial T}{\partial t}, & r_{\rm NP} \le r, \ t \ge 0 \\ T(r, t = 0) = 0, & T(r = \infty, t) = T_{\infty} \\ k_{\rm NP} \frac{\partial T(r = r_{\rm NP}^-, t)}{\partial r} = k \frac{\partial T(r = r_{\rm NP}^+, t)}{\partial r} \end{cases}$$

$$(1)$$

where T(r,t) is the temperature profile, r is the distance from NP center and $r_{\rm NP}$ is the radius of NP, t is time, q_V is volumetric heat source inside the NP, $\alpha_{\rm NP}$ and α , and $k_{\rm NP}$, and k are thermal diffusivity and thermal conductivity for NP and water, respectively. Although an analytical solution to Eq. (1) can be derived by Laplace transform (Eq. (S2) available in the Supplemental Materials on the ASME Digital Collection), known as Goldenberg's analytical solution [31], the complexity of the expression makes it challenging to use in our analysis of NP array heating. Therefore, we first simplify Eq. (1) by assuming a constant heat flux at the NP-water interface

$$\begin{cases} \frac{1}{r^2} \frac{\partial}{\partial r} \left(r^2 \frac{\partial T}{\partial r} \right) = \frac{1}{\alpha} \frac{\partial T}{\partial t}, & r_{\text{NP}} \le r, t \ge 0 \\ T(r, t = 0) = 0, & T(r = \infty, t) = T_{\infty} \\ k \frac{\partial T(r = r_{\text{NP}}, t)}{\partial r} 4\pi r_{\text{NP}}^2 + \frac{4}{3}\pi r_{\text{NP}}^3 q_v = 0 \end{cases}$$
 (2)

Equation (2) can be solved by Laplace transform [42]

$$\Delta T_{\text{single}} = T - T_{\infty} = \frac{q}{4\pi r k} \left[\text{erfc} \left(\frac{r - r_{\text{NP}}}{2\sqrt{\alpha t}} \right) - \exp\left(\frac{r - r_{\text{NP}}}{r_{\text{NP}}} + \frac{\alpha t}{r_{\text{NP}}^2} \right) \text{erfc} \left(\frac{r - r_{\text{NP}}}{2\sqrt{\alpha t}} + \frac{\sqrt{\alpha t}}{r_{\text{NP}}} \right) \right]$$
(3)

Note that by assuming a constant heat flux at the NP-water interface, we have neglected the heat capacity of the NP, thus

Eq. (3) only describes the temperature profile in the surrounding water during single NP heating with applied power q (heating power per NP, μ W). Since the heat capacity of the NP is small relative to that of the surrounding water, this approximation should only lead to a minor overestimation of the water temperature at the start of heating [42], yet expression in Eq. (3) is much simpler than Goldenberg's analytical solution to Eq. (1). Therefore, we will make use of Eq. (3) in our analysis of NP array heating.

Simulation for Nanoparticle Array Heating. The temperature rise in the NP array (ΔT_{array}) is estimated by the superposition of temperature rise of individual NP heating (ΔT_{single}) [44]

$$\Delta T_{\text{array}}(\mathbf{r},t) = \sum_{i=1}^{N} \Delta T_{\text{single},i}(|\mathbf{r} - \mathbf{r}_i|,t)$$
 (4)

where N is the total number of NPs, r_i is the location for ith NP, and the $\Delta T_{\rm single}$ is determined by the Goldenberg's analytical solution (Eq. (S2) available in the Supplemental Materials). Temperature profiles are calculated using MATLAB (2019b).

Results

Temperature Function for Nanoparticle Array Heating. Most applications of NP heating are based on multi-NP heating or NP cluster heating with thermal interactions among individual NPs. The diverse set of cluster geometries that multi-NP systems can assume makes it challenging to derive analytical descriptions of multi-NP heating. To circumvent this issue, we narrowed our scope to three representative NP cluster geometries (2D, 3D, and spherical NP clusters). We modeled the multi-NP heating via NP arrays with periodic lattices (Fig. 2, square and cubic lattice for 2D and 3D array, respectively, Fibonacci lattice for spherical array [49]) and assumed uniform heating power throughout the array.

For a circular shaped 2D NP array, the temperature rise at the center of the array ($\Delta T_{\rm 2D}$) can be estimated by

$$\Delta T_{2D}(t) = \sum_{i=1}^{N} \Delta T_{\text{single},i}(r_i, t)$$
 (5)

where r_i is the distance from the *i*th NP to the center of NP array. Figure 3(a) shows that, when the interparticle distance, p, is small

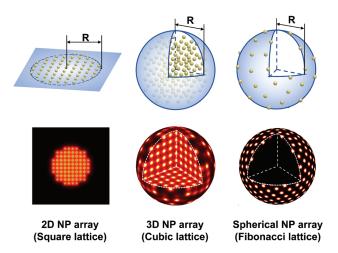


Fig. 2 Schematic illustrations of representative NP array geometries: 2D NP array with square lattice, 3D NP array with cubic lattice, spherical NP array with Fibonacci lattice. For 2D and 3D NP arrays, *R* represents the size of the NP array; for the spherical NP array, *R* represents the size of the sphere.

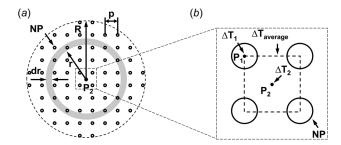


Fig. 3 Schematic illustrations of theoretical model: (a) Temperature function for 2D NP array is derived by transforming superposition into integration. (b) Representative locations and temperatures in the center lattice of the NP array. P_1 is located in NP and P_2 is located at the midpoint between NPs.

relative to the size of the array, R, (i.e., $R/p \gg 1$), summation in Eq. (5) can be estimated by an integration

$$\Delta T_{2D}(R,t) = \int_{r=0}^{r=R} \Delta T_{\text{single}}(r,t) \cdot 2\pi r \rho_{NP} \cdot dr$$
 (6)

where *R* is the size of the NP array (Figs. 2 and 3(*a*)) and $\rho_{\rm NP}$ is the NP concentration (μ m⁻² for 2D and spherical NP array, μ m⁻³ for 3D NP array). Substitute Eq. (3) into Eq. (6) gives

$$\Delta T_{2D} = \frac{q\rho_{\rm NP}}{2k} \left[R \cdot \operatorname{erfc}\left(\frac{R}{2\sqrt{\alpha t}}\right) + \frac{2\sqrt{\alpha t}}{\pi} \left(1 - \exp\left(\frac{-R^2}{4\alpha t}\right)\right) \right]$$

$$+ r_{\rm NP} \frac{q\rho_{\rm NP}}{2k} \cdot \left\{ \exp\left(\frac{R}{r_{\rm NP}} + \frac{\alpha t}{r_{\rm NP}^2}\right) \operatorname{erfc}\left(\frac{R}{2\sqrt{\alpha t}} + \frac{\sqrt{\alpha t}}{r_{\rm NP}}\right) \right.$$

$$- \exp\left(\frac{\alpha t}{r_{\rm NP}^2}\right) \operatorname{erfc}\left(\frac{\sqrt{\alpha t}}{r_{\rm NP}}\right) + \operatorname{erfc}\left(\frac{R}{2\sqrt{\alpha t}}\right) - 1 \right\}$$

$$(7)$$

Since the size of individual NP (r_{NP}) is minimal compared with that of the NP array ($R \gg r_{NP}$), thus we ignored the second term of the righthand side of Eq. (7), and it leads to Eq. (8) (Table 1).

of the righthand side of Eq. (7), and it leads to Eq. (8) (Table 1). Equation (8) describes temperature rise at the center point of a 2D NP array. We validated Eq. (8) by comparing it with simulation results. Notably, NP array heating with a large interparticle distance and a short heating time can result in a heterogeneous temperature profile (Fig. S1 available in the Supplemental

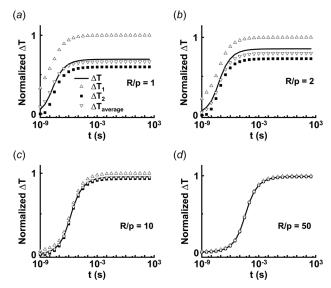


Fig. 4 Validation of the temperature function for 2D NP array heating: Comparing the function with solution of superposition results. The results from superposition are calculated based on Goldenberg's analytical solution for single NP heating (Eq. (S2) available in the Supplemental Materials), $r_{\rm NP} = 15$ nm. The size of the NP array (R) comparing with interparticle distance (p) is (a) R/p = 1, (b) R/p = 2, (c) R/p = 10, and (d) R/p = 50.

Materials on the ASME Digital Collection), i.e., confined heating. Therefore, we compared Eq. (8) to three representative ΔT values computed from numerical simulation of superposition (Figs. 3(b) and S1 available in the Supplemental Materials): ΔT_1 , ΔT_2 , and $\Delta T_{\text{average}}$, which correspond to the temperature rise inside an NP (at P1), the midpoint between NPs (at P2), and the average throughout central lattice, respectively. Figure 4 shows that Eq. (8) accurately describes the temperature rise especially for $\Delta T_{\text{average}}$, even for small NP arrays (R/p=1). These results confirm the accuracy of Eq. (8).

Following a similar process, we derived temperature functions for the 3D NP array and spherical NP array (Table 1, Eqs. (9) and (10)). Figure S2 available in the Supplemental Materials shows that results from Eqs. (9) and (10) are in good agreement with simulation results, which confirms the accuracy. Considering the

Table 1 Temperature functions for 2D, 3D, and spherical NP arrays

NP array geometry	Location	Temperature function	
2D NP array	Center point	$\Delta T_{2D} = \frac{q\rho_{\rm NP}}{2k} \left[R \cdot \operatorname{erfc}\left(\frac{R}{2\sqrt{\alpha t}}\right) + 2\sqrt{\frac{\alpha t}{\pi}} \left(1 - \exp\left(\frac{-R^2}{4\alpha t}\right)\right) \right]$	(8)
3D NP array	Center point	$\Delta T_{3D} = \frac{q\rho_{\rm NP}}{2k} \left[R^2 \cdot \operatorname{erfc}\left(\frac{R}{2\sqrt{\alpha t}}\right) - 2\sqrt{\frac{\alpha t}{\pi}} R \cdot \exp\left(\frac{-R^2}{4\alpha t}\right) + 2\alpha t \cdot \operatorname{erf}\left(\frac{R}{2\sqrt{\alpha t}}\right) \right]$	(9)
Spherical NP array On spherical surface		$\Delta T_{\text{SPH},s} = \frac{q\rho_{\text{NP}}}{k} \left[R \cdot \operatorname{erfc}\left(\frac{R}{\sqrt{\alpha t}}\right) + \sqrt{\frac{\alpha t}{\pi}} \left(1 - \exp\left(\frac{-R^2}{\alpha t}\right)\right) \right]$	(10)
	Center point	$\Delta T_{\text{SPH},c} = \frac{q\rho_{\text{NP}}}{k} \left[R \cdot \operatorname{erfc}\left(\frac{R - r_{\text{NP}}}{\sqrt{\alpha t}}\right) - R \cdot \exp\left(\frac{R - r_{\text{NP}}}{r_{\text{NP}}} + \frac{\alpha t}{r_{\text{NP}}^2}\right) \operatorname{erfc}\left(\frac{R - r_{\text{NP}}}{2\sqrt{\alpha t}} + \frac{\sqrt{\alpha t}}{r_{\text{NP}}}\right) \right] $	(11)

identical distance from NPs on the spherical surface to the center point, the temperature rise at the center point of a spherical NP array heating is obtained via multiplying Eq. (3) by the total number of NPs (N).

A close inspection shows that Eqs. (8)–(11) can be rewritten into a similar mathematical form

$$\Delta T = \frac{1}{2k} \cdot \underbrace{q\rho_{\text{NP}}}_{\text{Energy intensity term}} \cdot \underbrace{f(R,t)}_{\text{Spatiotemporal term}}$$
 (12)

where $q\rho_{\rm NP}$ serves as energy intensity term, and f(R,t) is the spatiotemporal diffusion term. Equation (12) reveals the underlying principle for transient NP array heating: temperature rise is the product of the linear energy intensity term, which is determined by heating power per NP and NP concentration, and a nonlinear spatiotemporal term, which is dependent on the NP array geometry and heating time.

The simple analytical solutions (Eqs. (8)-(11)) provide a method for further analysis on transient heating of NP arrays as well as useful expressions to estimate the temperature rise of representative NP array heating, alleviating the need to run heavy numerical simulations. For example, Eq. (8) can be used to estimate temperature rise for lithographically fabricated NP heating with repeated 2D lattice [37]. Similarly, Eq. (9) is useful in estimating temperature rise for photothermal therapy (PTT) or photothermal catalysis where free suspension of NPs in an aqueous solution can be treated as a 3D NP array [5,9,19].

Application of Nanoparticle Array Heating to Reach a Specified Temperature Change. The spatiotemporal scale of the NP array heating is often crucial for its applications. As an example, for PTT or plasmonic photothermal therapy, precise control of the heating range is necessary for effective tumor destruction while avoiding healthy tissue damage [7,50]. On the other hand, a specific temperature threshold is required to trigger a biological or chemical response. With these considerations, we analyzed the NP array heating from an alternative perspective: what are the necessary conditions for a specific temperature rise? Therefore, we analyzed the critical NP array size and critical heating time for a specific temperature rise.

We started with defining the target temperature rise (ΔT_{target}) for a specific application, such as activating thermally sensitive ion channels or triggering tumor cell necrosis [25,27]. To evaluate the necessary conditions for ΔT_{target} , we rewrite Eq. (12) into

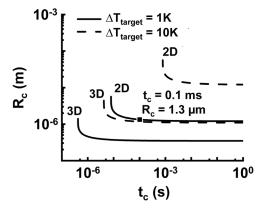


Fig. 5 Critical size of 2D and 3D NP arrays for specific temperature rise: Critical NP array size Rc and in terms of heating time t_c for 2D and 3D NP arrays. NP concentration ($\rho_{\rm NP}$): 100 $\mu{\rm m}^{-2}$ for 2D array and 1000 $\mu{\rm m}^{-3}$ for 3D array; heating power (q): 10 nW/

$$f(R_c, t_c) = \Delta T_{\text{target}} \cdot \frac{2k}{q\rho_{\text{NP}}}$$
 (13)

where R_c and t_c are critical NP array size and critical heating time, respectively. For a specific ΔT_{target} and energy intensity $(q\rho_{\text{NP}})$, Eq. (13) describes a combination of critical NP array size (R_c) and heating time (t_c) to reach the specified temperature increase. In other words, for each heating time (t_c) , a critical NP array size (R_c) can be determined (Fig. 5) and is the minimal NP array size to reach ΔT_{target} under the specific heating time (t_c). Similarly, for a given NP array size (R_c) , t_c represents the minimal heating time to reach ΔT_{target} . For example, Fig. 5 shows that at least a 2D NP array with $1.3 \,\mu \text{m}$ in diameter is needed to reach 1 K temperature rise under 1 ms heating ($\rho_{\rm NP} = 100 \, \mu {\rm m}^{-2}$, $q = 10 \, {\rm nW/NP}$). Furthermore, the NP array size (R_c) reaches an asymptotic

value when t_c goes to infinity, i.e., under the steady-state (s.s.)

$$R_{c,s.s.} = \begin{cases} \frac{2k}{q\rho_{\text{NP}}} \cdot \Delta T_{\text{target}}, \ 2D \ NP \ array \\ \sqrt{\frac{2k}{q\rho_{\text{NP}}}} \cdot \Delta T_{\text{target}}, \ 3D \ NP \ array \end{cases}$$
(14)

Equation (14) and Fig. 6(a) show the smallest array size to reach the required temperature change (ΔT_{target}) under the steadystate. Similarly, a larger-sized NP array (R_c) can lead to a shorter heating time (t_c) . With an infinitely large array, a minimum heating time can be obtained to reach the specified temperature change $(\Delta T_{\rm target})$

$$t_{c, \, \text{inf.}} = \begin{cases} \frac{\pi k^2}{\alpha} \left(\frac{1}{q \rho_{\text{NP}}} \cdot \Delta T_{\text{target}} \right)^2, \, 2D \, NP \, array \\ \frac{k}{\alpha} \cdot \frac{1}{q \rho_{\text{NP}}} \cdot \Delta T_{\text{target}}, \, 3D \, NP \, array \end{cases}$$
(15)

Equation (15) and Fig. 6(b) show that minimal heating time with an infinite sized NP array $(t_{c,inf.})$ is determined by energy intensity. For example, Fig. 6(b) shows that for 3D NP array heating with energy intensity at 1 pW/ μ m⁻³, the heating time should be at least 1 s to reach a 1 K temperature rise.

Thermal Resolution. Our analysis of the critical NP array size (R_c) can be applied to define a "thermal resolution." An emerging application involves activating neurons in the retina to restore vision [24]. Dasha et al. showed that, when excited by nearinfrared radiation, the plasmonic gold nanorods attached to the retina serve as nanoheaters, and can thermally activate the TRPV1 channel. The heating of nanorods inside the light spot can be modeled as 2D NP array heating, where the size of the NP array (R) is

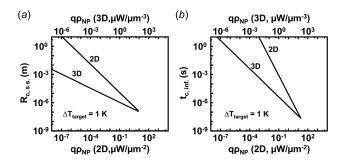


Fig. 6 Critical size under steady-state (a) and critical heating time with infinite NPs (b) for 2D and 3D NP arrays in terms of energy intensity. Unit for energy intensity is $\mu W/\mu m^{-2}$ for 2D NP arrays and $\mu W/\mu m^{-3}$ for 3D NP arrays.

determined by the size of the light spot projected on the retina. One of the key questions is the resolution for this application from the heat transfer's perspective. As such, we define a "thermal resolution" based on the critical size of the NP array heating (R_c) . Here we assume R_c sized NP array heating is necessary to reach the temperature threshold for TRPV1 activation. Figure 7 shows the minimal distance $(D=2R_c)$ at which two R_c sized hot spots can be distinguished from each other. When $D < 2R_c$, the merged hot spots (Figs. 7(b) and 7(c)) will lead to an overlap of TRPV1 activation, ending up with a single "sensed" light spot. Consequently, R_c serves as the thermal resolution.

As mentioned above, the critical NP array size under steady-state ($R_{c,s,s}$) shows an upper limit for thermal resolution. Equation (14) and Fig. 6(a) show that the $R_{c,s,s}$ is determined by the energy intensity ($q\rho_{\rm NP}$) with higher energy intensity resulting in greater possible thermal resolution (smaller $R_{c,s,s}$). There are several significant implications of this result. Recently, various studies have focused on applications with localized NP heating, from targeted tumor thermal treatment [5] to neuron modulation [24], and molecular hyperthermia [29]. Our analysis shows that the thermal resolution gives a spatial limit when designing specific micro or nanoheating patterns and that the energy intensity is the key for greater thermal resolution. As an example, Fig. 6(a) shows that energy intensity ($q\rho_{\rm NP}$) of 0.1 μ W/ μ m⁻³ is necessary for selective cellular heating ($R_c \sim 1$ –10 μ m) with 3D NP array.

Dimensionless Parameter Characterizing Confined Heating. In the Thermal Resolution section, we discussed the degree of thermal confinement in the perspective of necessary conditions for an NP array to reach the $\Delta T_{\rm target}$ and developed the idea of thermal

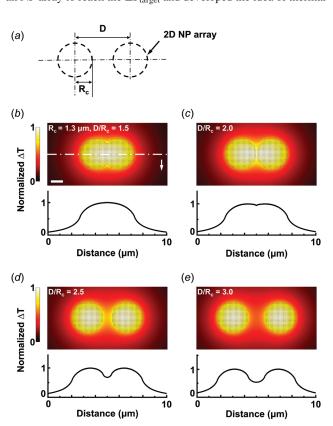


Fig. 7 Schematic illustration (a) of interarray distance (D), and temperature profiles (b–e) for two 2D NP arrays with different D: $R_c=1.3~\mu\text{m},~t_c=1~\text{ms},~r_{\text{NP}}=15~\text{nm},~\rho_{\text{NP}}=100~\mu\text{m}^{-2},~q=10~\text{nW}/\text{NP},~D=(b)~1.95~\mu\text{m}~(c)~2.6~\mu\text{m}~(d)~3.25~\mu\text{m}~(e)~3.9~\mu\text{m}.$ Scalebar represents 1 $\mu\text{m}.$ When $D>2R_c,$ two distinguishable hot spots corresponding to the NP arrays are observed, while $D\leq2R_c,$ the two hot spots merged and can no longer be distinguished as individuals.

resolution. In this section, we will focus on thermal confinement inside the NP array, i.e., heating overlap among NPs in an NP array. One of the basic ideas for characterizing the degree of confined heating is to compare the thermal diffusion distance with the interparticle distance. Kang et al. Developed a dimensionless parameter based on comparing the thermal diffusion distance of single NP heating with the interparticle distance [30], which quantifies the heating overlap between two NPs. Despite this, parameters that consider the ensemble effect among NPs in an NP array would greatly advance our understanding of the heating modes. Here we developed a set of dimensionless parameters to characterize the confined heating by quantifying the thermal diffusion distance in an NP array.

According to Eqs. (8)–(11), larger NP array size (R) gives greater $\Delta T(R,t)$, and when R tends to infinity, a heating time-dependent $\Delta T_{\rm inf.}(t)$ can be expressed as follows:

$$\Delta T_{\rm inf.} = \begin{cases} \frac{q\rho_{\rm NP}}{k} \sqrt{\frac{\alpha t}{\pi}}, 2D\,NP\,array\\ \frac{q\rho_{\rm NP}}{k} \alpha t, 3D\,NP\,array \end{cases}$$
(16)

Figure 8(a) shows $\Delta T(R,t)$ in terms of R for a specific heating time: Larger R results in greater $\Delta T(R,t)$, which asymptotically reaches $\Delta T_{\inf}(t)$ as R tends to infinity. Here a critical $R_{\operatorname{diff}}(t)$ is defined as when $\Delta T(R,t)$ approximates $\Delta T_{\inf}(t)$ (Fig. 8(a)). As shown in Fig. 8(a), $R_{\operatorname{diff}}(t)$ divides the R into R-limiting zone $(R < R_{\operatorname{diff}}(t))$, where $\Delta T(R,t)$ increases significantly with R, and the t-limiting zone $(R \ge R_{\operatorname{diff}}(t))$, where $\Delta T(R,t)$ approximates $\Delta T_{\inf}(t)$ and no obvious increase for $\Delta T(R,t)$ is observed. The sharp contrast between these two zones demonstrates that $R_{\operatorname{diff}}(t)$ serves as the thermal diffusion distance in an NP array, where only NPs within the distance of $R_{\operatorname{diff}}(t)$ impact the temperature change at the center point. It should be noticed that $R_{\operatorname{diff}}(t)$ is time-dependent, where an increasing t results in larger $R_{\operatorname{diff}}(t)$ (Fig. 8(b)).

Given the above insight into the thermal diffusion in an NP array, we can quantify the heating overlap and develop a

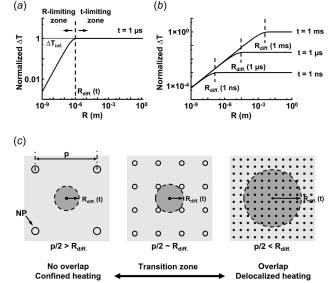


Fig. 8 Thermal diffusion distance in NP array $(R_{\rm diff.})$. (a) ΔT in terms of R with a specific heating time $(t=1~\mu {\rm s})$. When $\Delta T \sim \Delta T_{\rm inf.}$, a critical NP array size can be observed $(R_{\rm diff.})$. When $R < R_{\rm diff.}$, increasing R results in a significant increase of ΔT , while for $R > R_{\rm diff.}$, ΔT is approximately equal to $\Delta T_{\rm inf.}$ (B) Thermal diffusion distance in NP array $(R_{\rm diff.})$ with different heating time (f). (C) Heating overlap among NPs can be characterized by comparing interparticle distance (p) with $R_{\rm diff.}$

Table 2 Dimensionless parameters characterizing the heating overlap

NP array geometry	Description	Dimensionless parameter
2D NP array	Heating overlap between NPs	$\zeta_{2D} = \frac{\Delta T\left(\frac{p}{2}, t\right)}{\Delta T_{\text{inf.}}(t)} = \frac{\left(\frac{p}{2}\right) \cdot \operatorname{erfc}\left(\frac{p}{4\sqrt{\alpha t}}\right) + 2\sqrt{\frac{\alpha t}{\pi}}\left(1 - \exp\left(\frac{-p^2}{16\alpha t}\right)\right)}{2\sqrt{\frac{\alpha t}{\pi}}} $ (17)
3D NP array		$(-1)^2$
		$\zeta_{3D} = \frac{\Delta T(\frac{p}{2}, t)}{\Delta T_{\text{inf.}}(t)} = \frac{\left(\frac{p}{2}\right)^2 \cdot \operatorname{erfc}\left(\frac{p}{4\sqrt{\alpha t}}\right) - \sqrt{\frac{\alpha t}{\pi}} p \cdot \exp\left(\frac{-p^2}{16\alpha t}\right) + 2\alpha t \cdot \operatorname{erf}\left(\frac{p}{4\sqrt{\alpha t}}\right)}{2\alpha t} $ (18)
Spherical NP array	Heating overlap between NPs along the spherical surface	$ \zeta_{\text{SPH,s}} = \frac{\Delta T\left(\frac{p}{2}, t\right)}{\Delta T_{\text{inf.}}(t)} = \frac{1}{2} p \sqrt{\frac{\pi}{\alpha t}} \cdot \operatorname{erfc}\left(\frac{p}{2\sqrt{\alpha t}}\right) + 1 - \exp\left(\frac{-p^2}{4\alpha t}\right) $ $ \rho_{\text{NP}} = \frac{N}{4\pi R^2}, p = \sqrt{\frac{1}{\rho_{NP}}} $ (19)
	Heating overlap between spherical surface and center point	$\eta_{\text{SPH},c} = 1 - \frac{\Delta T_{\text{SPH},c}}{\Delta T_{\text{SPH},s}} = 1 - \frac{R \cdot \left[\text{erfc} \left(\frac{R - r_{\text{NP}}}{\sqrt{\alpha t}} \right) - \exp \left(\frac{R - r_{\text{NP}}}{r_{\text{NP}}} + \frac{\alpha t}{r_{\text{NP}}^2} \right) \text{erfc} \left(\frac{R - r_{\text{NP}}}{2\sqrt{\alpha t}} + \frac{\sqrt{\alpha t}}{r_{\text{NP}}} \right) \right]}{R \cdot \text{erfc} \left(\frac{R}{\sqrt{\alpha t}} \right) + \sqrt{\frac{\alpha t}{\pi}} \left[1 - \exp \left(\frac{-R^2}{\alpha t} \right) \right]} $ (20)

dimensionless parameter by comparing the $R_{\rm diff}(t)$ with interparticle distance (p) (Fig. 8(c)): if $p/2 \gg R_{\rm diff}(t)$ ($2R_{\rm diff}/p \ll 1$), the heating overlap is minimal and confined heating is established; whereas if $p/2 \ll R_{\rm diff}(t)$ ($2R_{\rm diff}/p \gg 1$), significant heating overlap leads to delocalized heating. However, there are two key problems for developing a dimensionless parameter based on this idea:

- (1) The mathematical definition of $R_{\rm diff.}$ is not clear. As mentioned above, $R_{\rm diff.}$ is defined as when $\Delta T(R,t) \sim \Delta T_{\rm inf.}(t)$, yet the approximation is not a clear and a slight change of the approximation (i.e., $\Delta T/\Delta T_{\rm inf.} = 0.9$ or $\Delta T/\Delta T_{\rm inf.} = 0.99$) can result in significant difference in $R_{\rm diff.}$ as well as in $p/2R_{\rm diff.}$ This makes it challenging to determine $R_{\rm diff.}$ mathematically.
- (2) No explicit expression for $R_{\rm diff}$. Since $R_{\rm diff}$ is defined by the behavior of $\Delta T(R,t)$, $R_{\rm diff}$ could only be expressed implicitly by Eq. (13).

To overcome these limitations, we quantified the heating overlap from an alternative perspective: here we define a $R'_{\rm diff.} = p/2$, and by substituting this $R'_{\rm diff.}$ into Eq. (8) or (9), $\Delta T(R'_{\rm diff.},t)$ (or $\Delta T(p/2,t)$) can be determined explicitly. And by comparing this $\Delta T(R'_{\rm diff.},t)$ with $\Delta T_{inf.}(t)$, we can quantify the relation between $R_{\rm diff.}$ and p, i.e., characterizing the heating overlap. Based on this idea, we defined a set of dimensionless parameters ($\zeta(p,t)$) to characterize the heating overlap among NPs in 2D and 3D NP arrays (Table 2). Figure 9 shows that ζ nicely characterizes the degree of heating overlap among NPs and captures the transition from confined heating to delocalized heating: $\zeta \to 1$ indicates minimal heating overlap and $\zeta \to 0$ indicates heating overlap between NPs.

For the spherical NP array, the dimensionless parameter $(\zeta_{\text{SPH},s}(p,t))$ is defined to characterize the heating overlap along the spherical surface by following a similar mathematical process (Table 2, Eq. (19)). Another parameter $(\eta_{\text{SPH},c}(R,t))$ is defined to characterize the heating overlap between the spherical surface and

center point by comparing the temperature rise on the spherical surface with that at the center point (Table 2, Eq. (20)). A further inspection shows that the heating time (t) corresponding to $\zeta_{\text{SPH},s} = 0.5$ is constantly shorter than that corresponding to $\eta_{\text{SPH},c} = 0.5$ (Fig. 10(a)), indicating heating overlap first occurs along the spherical surface, and then further delocalizes throughout the volume inside the sphere (Fig. 10(b)), i.e., there is a window where heating is confined to the spherical surface with minimal heating inside the sphere; this effect may be particularly relevant when heating NPs arrayed across the surface of a nanovesicle or living cell.

The dimensionless parameters we have derived are a significant step forward in differentiating confined heating from delocalized

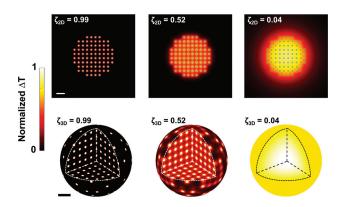


Fig. 9 Dimensionless parameter (ζ) characterizes the heating overlap and the transition from confined heating to delocalized heating in 2D and 3D NP array. When $\zeta\sim 1$, confined heating is observed, whereas $\zeta\sim 0$ heating overlap leads to delocalized heating. Scalebar represents 200 nm, $r_{\rm NP}=15$ nm.

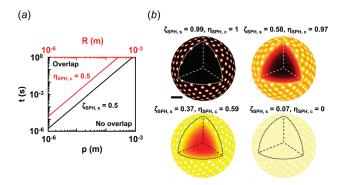


Fig. 10 Dimensionless parameters (ζ and η) characterize heating overlap and the transition from confined heating to delocalized heating for spherical NP array: (a) critical line for $\zeta_{\rm SPH,s}=0.5$ and $\eta_{\rm SPH,c}=0.5$. The critical line for $\eta_{\rm SPH,c}=0.5$ is constantly above the line for $\zeta_{\rm SPH,s}=0.5$, indicating delocalized heating first occurs along the spherical surface. (b) ΔT profile for spherical arrays. $\zeta_{\rm SPH,s}$ and $\eta_{\rm SPH,c}$ characterize the degree of heating overlap alone the spherical surface and inside the sphere. Scalebar represents 200 nm, $r_{NP}=15$ nm.

heating in the case of transient NP array heating, as they allow quantifying the effect of thermal diffusion for a specific NP array. Recently, great progress has been made in developing novel applications based on nanoscale localized NP heating, such as molecular hyperthermia and neuron modulation [24,29]. We anticipate that our work here advances the fundamental understanding of NP heating that underlies such applications, and provides a muchneeded description of NP array heating that can be used when optimizing the spatiotemporal evolution of the temperature profile in these applications.

Discussion

Physical Meaning of the Dimensionless Parameter (ζ). The physical meaning of the ζ requires further discussion. Based solely on the mathematical expressions, ζ represents the ratio of the temperature rise of a finite sized NP array to the temperature rise of an infinite sized NP array. However, neither of these descriptions truly represents the array we are analyzing. If we consider how ζ was derived, the physical meaning of ζ can be interpreted as a transformed ratio between the interparticle distance (p) and the thermal diffusion distance ($R_{\text{diff.}}$). In other words, instead of directly comparing the two distances (p and $R_{\text{diff.}}$), we substituted the distance into the spatiotemporal term (Eq. (12)) and compared the results. In this case, the result from Eq. (12) should be considered as a transformed distance based on the spatiotemporal property of the NP array rather than the temperature rise. This interpretation is reasonable for ζ_{2D} and ζ_{3D} . However, considering that the $R_{\text{diff.}}$ Represents the critical radius of the sphere for a spherical NP array, instead of the thermal diffusion along the spherical surface, we cannot apply this interpretation for $\zeta_{SPH,s}$

Relations Between Thermal Resolution (R_c) and Dimensionless Parameter (ζ). Both thermal resolution R_c and dimensionless parameter ζ focus on the spatiotemporal distribution of the temperature profile. The thermal resolution is derived from an externally imposed target value of the temperature rise, which in turn leads to corresponding limits on the spatial and temporal scale of the NP array heating. In contrast, the dimensionless parameter reflects the internal shape of the temperature profile within an NP array, regardless of the magnitude of the temperature.

Conclusion

In this work, we aimed at a comprehensive analysis of the transient heating process for NP arrays by: (i) Deriving analytical temperature functions to predict the temperature rise for 2D, 3D,

and spherical NP arrays, (ii) analyzing the conditions necessary to yield a specific temperature rise and developing the corresponding idea of thermal resolution, (iii) developing a set of dimensionless parameters that characterize the transition from confined heating (minimal heating overlap) to delocalized heating (significant heating overlap). In the case of the spherical NP array, our analysis revealed a window where there is substantial heating along the spherical surface but minimal heating inside the sphere, which is particularly relevant when designing applications based on heating NPs arrayed across the surface of nanovesicles or living cells. This work provides an in-depth understanding of the spatiotemporal evolution of temperature for NP array heating and provides guidance for designing approaches based on this form of NP heating.

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Nomenclature

Roman Letters

D = inter array distance, m

k =thermal conductivity of water, W m⁻² K⁻¹

 $k_{\rm NP}$ = thermal conductivity of nanoparticle, W m⁻² K⁻¹

N = total number of nanoparticles in an array

p = interparticle distance, m

q = heating power per nanoparticle, W

 $q_v = \text{volumetric heating source, W m}^{-3}$

r =distance from the center, m

r = location vector

R = radius of NP array, m

 $r_{\rm NP}$ = radius of nanoparticle, m

 R_c = spatial thermal resolution, M

 $R_{c,s,s}$ = spatial thermal resolution under steady-state, M

 $R_{\text{diff.}}$ = thermal diffusion distance, M

 $R'_{\text{diff.}}$ = substitute thermal diffusion distance, M

t = time, s

T = temperature, K

 t_c = critical heating time, s

 $t_{c, \text{inf.}} = \text{critical heating time with infinite sized nanoparticle}$ array heating, s

 T_{∞} = room temperature, K

 ΔT = temperature rise, K

 $\Delta T_{\text{average}}$ = average temperature throughout the center lattice in a nanoparticle array, K

 $\Delta T_{\rm inf.} =$ temperature rise with an infinite sized nanoparticle

array heating K

 $\Delta T_{\rm single}$ = temperature rise of single nanoparticle heating, K

 $\Delta T_{\rm SPH}$ = temperature rise of spherical nanoparticle array

heating, K

 $\Delta T_{target} =$ Specific temperature rise threshold for an application, K

 ΔT_1 = temperature rise in the nanoparticle of the center lattice, K

 ΔT_2 = temperature rise at the mid-point between nanoparticles of the center lattice, K

 ΔT_{2D} = temperature rise of 2D nanoparticle array heating, K ΔT_{3D} = temperature rise of 3D nanoparticle array heating, K

Greek Symbols

 α = thermal diffusivity of water, m² s⁻¹

 α_{NP} = thermal diffusivity of nanoparticle, $m^2 s^{-1}$

 $\zeta_{\text{SPH},s} = \text{dimensionless parameter for spherical nanoparticle}$ array, on a spherical surface

 $\zeta_{2D} =$ dimensionless parameter for 2D nanoparticle array ζ_{3D} = dimensionless parameter for 3D nanoparticle array

 $\eta_{\text{SPH},c} = \text{dimensionless parameter for spherical nanoparticle}$

array, at the center of the sphere

 $\rho_{\rm NP} = {\rm nanoparticle} \; {\rm concentration}, \, {\rm m}^{-2} \; ({\rm for} \; {\rm 2D} \; {\rm and} \; {\rm spherical} \;$ array), m^{-3} (for 3D array)

Abbreviations

diff. = diffusion

 \inf = \inf

NP = nanoparticle

PTT = photothermal therapy

s.s. = steady-state

SPH = spherical

TRPV1 = transient receptor potential cation channel, subfamily V. member 1

References

- [1] Park, J., Huang, J., Wang, W., Murphy, C. J., and Cahill, D. G., 2012, "Heat Transport Between Au Nanorods, Surrounding Liquids, and Solid Supports," J.
- Phys. Chem. C, 116(50), pp. 26335–26341.
 [2] Qin, Z., and Bischof, J. C., 2012, "Thermophysical and Biological Responses of Gold Nanoparticle Laser Heating," Chem. Soc. Rev., 41(3), pp. 1191–1217.
- [3] Deatsch, A. E., and Evans, B. A., 2014, "Heating Efficiency in Magnetic Nanoparticle Hyperthermia," J. Magn. Magn. Mater., 354, pp. 163-172
- [4] Pustovalov, V. K., 2005, "Theoretical Study of Heating of Spherical Nanoparticle in Media by Short Laser Pulses," Chem. Phys., 308(1-2), pp. 103-108.
- [5] Huang, X., Jain, P. K., El-Sayed, I. H., and El-Sayed, M. A., 2008, "Plasmonic Photothermal Therapy (PPTT) Using Gold Nanoparticles," Lasers Med. Sci., 23(3), pp. 217-228.
- [6] Hu, C. M., Aryal, S., and Zhang, L., 2010, "Nanoparticle-Assisted Combination Therapies for Effective Cancer Treatment," Ther. Deliv., 1(2), pp. 323–334.
- [7] Riley, R. S., and Day, E. S., 2017, "Gold Nanoparticle-Mediated Photothermal Therapy: Applications and Opportunities for Multimodal Cancer Treatment,' Wiley Interdiscip. Rev. Nanomed. Nanobiotechnol., 9(4), p. e1449.
- [8] Zhi, D., Yang, T., O'hagan, J., Zhang, S., and Donnelly, R. F., 2020, 'Photothermal Therapy," J. Control. Release, 325, pp. 52-71.
- [9] Richardson, H. H., Carlson, M. T., Tandler, P. J., Hernandez, P., and Govorov, A. O., 2009, "Experimental and Theoretical Studies of Light-to-Heat Conversion and Collective Heating Effects in Metal Nanoparticle Solutions," Nano Lett., **9**(3), pp. 1139–1146.
- [10] Niikura, K., Iyo, N., Matsuo, Y., Mitomo, H., and Ijiro, K., 2013, "Sub-100 nm Gold Nanoparticle Vesicles as a Drug Delivery Carrier Enabling Rapid Drug Release Upon Light Irradiation," ACS Appl. Mater. Interfaces, 5(9), pp.
- [11] Singh, R., and Lillard, J. W., Jr, 2009, "Nanoparticle-Based Targeted Drug Delivery," Exp. Mol. Pathol., 86(3), pp. 215-223.
- [12] Goodman, A. M., Hogan, N. J., Gottheim, S., Li, C., Clare, S. E., and Halas, N. J., 2017, "Understanding Resonant Light-Triggered DNA Release From Plasmonic Nanoparticles," ACS Nano, 11(1), pp. 171-179.
- [13] Kang, H., Lee, G.-H., Jung, H., Lee, J. W., and Nam, Y., 2018, "Inkjet-Printed Biofunctional Thermo-Plasmonic Interfaces for Patterned Neuromodulation," ACS Nano, 12(2), pp. 1128–1138.
- [14] Fraire, J. C., Masseroni, M. L., Jausoro, I., Perassi, E. M., Diaz Anel, A. M., and Coronado, E. A., 2014, "Identification, Localization, and Quantification of Neuronal Cell Membrane Receptors With Plasmonic Probes: Role of Protein Kinase D1 in Their Distribution," ACS Nano, 8(9), pp. 8942–8958.
- [15] Li, W., and Chen, X., 2015, "Gold Nanoparticles for Photoacoustic Imaging," Nanomed. J., 10(2), pp. 299–320.
- [16] Mantri, Y., and Jokerst, J. V., 2020, "Engineering Plasmonic Nanoparticles for Enhanced Photoacoustic Imaging," ACS Nano, 14(8), pp. 9408–9422
- [17] Boyer, D., Tamarat, P., Maali, A., Lounis, B., and Orrit, M., 2002, "Photothermal Imaging of Nanometer-Sized Metal Particles Among Scatterers," Science, **297**(5584), pp. 1160–1163.
- [18] Russier, J., Oudjedi, L., Piponnier, M., Bussy, C., Prato, M., Kostarelos, K., Lounis, B., Bianco, A., and Cognet, L., 2017, "Direct Visualization of Carbon

- Nanotube Degradation in Primary Cells by Photothermal Imaging," Nanoscale, 9(14), pp. 4642-4645.
- [19] Mateo, D., Morlanes, N., Maity, P., Shterk, G., Mohammed, O. F., and Gascon, J., 2021, "Efficient Visible-Light Driven Photothermal Conversion of CO2 to Methane by Nickel Nanoparticles Supported on Barium Titanate," Adv. Funct. Mater., 31(8), p. 2008244.
- [20] Zhu, L., Gao, M., Peh, C. K. N., and Ho, G. W., 2018, "Solar-Driven Photothermal Nanostructured Materials Designs and Prerequisites for Evaporation and Catalysis Applications," Mater. Horiz., 5(3), pp. 323–343.
- [21] Adleman, J. R., Boyd, D. A., Goodwin, D. G., and Psaltis, D., 2009, "Heterogeneous Catalysis Mediated by Plasmon Heating," Nano Lett., 9(12), pp. 4417-4423.
- [22] Mornet, S., Vasseur, S., Grasset, F., Veverka, P., Goglio, G., Demourgues, A., Portier, J., Pollert, E., and Duguet, E., 2006, "Magnetic Nanoparticle Design for Medical Applications," Prog. Solid State Chem., 34(2-4), pp. 237-247.
- [23] Xiaohua, F., Fei, G., and Yuanjin, Z., 2015, "Photoacoustic-Based-Close-Loop Temperature Control for Nanoparticle Hyperthermia," IEEE Trans. Biomed. Eng., 62(7), pp. 1728–1737
- [24] Nelidova, D., Morikawa, R. K., Cowan, C. S., Raics, Z., Goldblum, D., Scholl, H. P., Szikra, T., Szabo, A., Hillier, D., and Roska, B., 2020, "Restoring Light Sensitivity Using Tunable Near-Infrared Sensors," Science, 368(6495), pp. 1108-1113.
- [25] Yao, J., Liu, B., and Qin, F., 2010, "Kinetic and Energetic Analysis of Thermally Activated TRPV1 Channels," Biophys. J., 99(6), pp. 1743–1753
- [26] Castillo, K., Diaz-Franulic, I., Canan, J., Gonzalez-Nilo, F., and Latorre, R., 2018, "Thermally Activated TRP Channels: Molecular Sensors for Temperature Detection," Phys. Biol., 15(2), p. 021001.
- [27] Brown, W. G., Needham, K., Begeng, J. M., Thompson, A. C., Nayagam, B. A., Kameneva, T., and Stoddart, P. R., 2020, "Thermal Damage Threshold of Neurons During Infrared Stimulation," Biomed. Opt. Exp., 11(4), pp. 2224-2234
- [28] Kang, P., Chen, Z., Nielsen, S. O., Hoyt, K., D'Arcy, S., Gassensmith, J. J., and Qin, Z., 2017, "Molecular Hyperthermia: Spatiotemporal Protein Unfolding and Inactivation by Nanosecond Plasmonic Heating,"
- [29] Kang, P., Li, X., Liu, Y., Shiers, S. I., Xiong, H., Giannotta, M., Dejana, E., Price, T. J., Randrianalisoa, J., Nielsen, S. O., and Qin, Z., 2019, "Transient Photoinactivation of Cell Membrane Protein Activity Without Genetic Modification by Molecular Hyperthermia," ACS Nano, 13(11), pp. 12487-12499.
- [30] Kang, P., Xie, C., Fall, O., Randrianalisoa, J., and Qin, Z., 2021, 'Computational Investigation of Protein Photoinactivation by Molecular Hyperthermia," ASME J. Biomech. Eng., 143(3), p. 031004. [31] Goldenberg, H., and Tranter, C., 1952, "Heat Flow in an Infinite Medium
- Heated by a Sphere," Br. J. Appl. Phys., 3(9), pp. 296–298.
- [32] Hastman, D. A., Melinger, J. S., Aragonés, G. L., Cunningham, P. D., Chiriboga, M., Salvato, Z. J., Salvato, T. M., Brown, C. W., Mathur, D., Medintz, I. Oh, E., and Díaz, S. A., 2020, "Femtosecond Laser Pulse Excitation of DNA-Labeled Gold Nanoparticles: Establishing a Quantitative Local Nanothermometer for Biological Applications," ACS Nano, 14(7), pp. 8570-8583.
- Nguyen, S. C., Zhang, Q., Manthiram, K., Ye, X., Lomont, J. P., Harris, C. B., Weller, H., and Alivisatos, A. P., 2016, "Study of Heat Transfer Dynamics From Gold Nanorods to the Environment Via Time-Resolved Infrared Spectroscopy," ACS Nano, 10(2), pp. 2144–2151. Gerasimov, V., Ershov, A., Karpov, S., Polyutov, S., and Semina, P., 2016,
- "Optimization of Photothermal Methods for Laser Hyperthermia of Malignant Cells Using Bioconjugates of Gold Nanoparticles," Colloid J., 78(4), pp. 435-442.
- [35] Baffou, G., and Rigneault, H., 2011, "Femtosecond-Pulsed Optical Heating of Gold Nanoparticles," Phys. Rev. B, 84(3), p. 035415.
- [36] Khlebtsov, B., Zharov, V., Melnikov, A., Tuchin, V., and Khlebtsov, N., 2006, "Optical Amplification of Photothermal Therapy With Gold Nanoparticles and Nanoclusters," Nanotechnology, 17(20), pp. 5167–5179.
- [37] Guler, U., Ndukaife, J. C., Naik, G. V., Nnanna, A. A., Kildishev, A. V., Shalaev, V. M., and Boltasseva, A., 2013, "Local Heating With Lithographically Fabricated Plasmonic Titanium Nitride Nanoparticles," Nano Lett., **13**(12), pp. 6078-6083
- [38] Yan, X., Liu, G., Xu, J., and Wang, S., 2018, "Plasmon Heating of One-Dimensional Gold Nanoparticle Chains," J. Sol. Energy, 173, pp.
- [39] Nemec, S., Kralj, S., Wilhelm, C., Abou-Hassan, A., Rols, M.-P., and Kolosnjaj-Tabi, J., 2020, "Comparison of Iron Oxide Nanoparticles in Photothermia and Magnetic Hyperthermia: Effects of Clustering and Silica Encapsulation on
- Nanoparticles' Heating Yield," Appl. Sci., 10(20), p. 7322.
 [40] Govorov, A. O., Zhang, W., Skeini, T., Richardson, H., Lee, J., and Kotov, N. A., 2006, "Gold Nanoparticle Ensembles as Heaters and Actuators: Melting and Collective Plasmon Resonances," Nanoscale Res. Lett., **1**(1), pp. 84–90.
- [41] Baffou, G., Quidant, R., and Girard, C., 2009, "Heat Generation in Plasmonic Nanostructures: Influence of Morphology," Appl. Phys. Lett., 94(15), o. 153109.
- [42] Keblinski, P., Cahill, D. G., Bodapati, A., Sullivan, C. R., and Taton, T. A., 2006, "Limits of Localized Heating by Electromagnetically Excited Nanoparticles," J. Appl. Phys., 100(5), p. 054305.
- Baffou, G., Quidant, R., and Girard, C., 2010, "Thermoplasmonics Modeling:
- A Green's Function Approach," Phys. Rev. B, **82**(16), p. 165424. [44] Baffou, G., Berto, P., Bermudez Urena, E., Quidant, R., Monneret, S., Polleux, J., and Rigneault, H., 2013, "Photoinduced Heating of Nanoparticle Arrays,"

- ACS Nano, 7(8), pp. 6478-6488.
- [45] Tay, Z. W., Chandrasekharan, P., Chiu-Lam, A., Hensley, D. W., Dhavalikar, R., Zhou, X. Y., Yu, E. Y., Goodwill, P. W., Zheng, B., Rinaldi, C., and Conolly, S. M., 2018, "Magnetic Particle Imaging-Guided Heating In Vivo Using Gradient Fields for Arbitrary Localization of Magnetic Hyperthermia Therapy," ACS Nano, 12(4), pp. 3699–3713.
 Jauffred, L., Samadi, A., Klingberg, H., Bendix, P. M., and Oddershede, L. B., 2019, "Plasmonic Heating of Nanostructures," Chem. Rev., 119(13), pp. 8087–8130.
- [47] Qin, Z., Etheridge, M., and Bischof, J. C., "Nanoparticle Heating: Nanoscale to Bulk Effects of Electromagnetically Heated Iron Oxide and Gold for
- Biomedical Applications," Proceedings of Energy-Based Treatment Tissue and Assessment VI, International Society for Optical Photonics, **7901**, San Francisco, CA, Feb. 23, p. 79010C.
- [48] Kaczmarek, K., Hornowski, T., Antal, I., Timko, M., and Józefczak, A., 2019, "Magneto-Ultrasonic Heating With Nanoparticles," J. Magn. Magn. Mater., **474**, pp. 400–405.
- [49] González, A., 2010, "Measurement of Areas on a Sphere Using Fibonacci and Latitude–Longitude Lattices," Math. Geosci., 42(1), pp. 49–64.
 [50] Chen, Z., Shan, X., Guan, Y., Wang, S., Zhu, J. J., and Tao, N., 2015, "Imaging
- Local Heating and Thermal Diffusion of Nanomaterials With Plasmonic Thermal Microscopy," ACS Nano, 9(12), pp. 11574–11581.